

Coordinate Attention UNet

Quoc An Dang and Duc Dung Nguyen

Computer Science and Engineering Faculty, Ho Chi Minh City University of Technology, Vietnam

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Abstract: In this paper, we propose an alternative architecture based on the UNet, which utilized the attention module. Our model solved the context loss and feature dilution caused by sampling operation of the UNet model using the enhancement ability of the attention. Further more, we applied one of the latest attention module named Coordinate Attention module to our model and proposed modification of this module to improve the effective of this module for Magnetic Resonance Imaging (MRI) scans.

1 INTRODUCTION

Gliomas brain tumor is the most aggressive malignant primary brain tumor. It mostly occur in adults having low survival rate (Tamimi and Juweid, 2017). For diagnosing the tumor, The traditional method is segmenting the Magnetic Resonance Imaging (MRI) by specialist, which is very costly and time consuming. Therefore the needed of an automated segment method arisen.

In recent years, many researchers working on the method to segmenting brain tumor. The work varied from the basic CNN model (Havaei et al., 2015) to the encoder-decoder architecture like UNet (Ronneberger et al., 2015), UNet++ (Zhou et al., 2018), VNet (Milletari et al., 2016), nnUNet (Isensee et al., 2018). Then in order to utilize the z-axis feature, many 3D model appeared like 3D UNet (Çiçek et al., 2016), 3D Dilated Multi-Fiber Network (Chen et al., 2019), 3D autoencoder regularization (Myronenko, 2018). And among the lots of research, UNet model still appeared to be one of the most typical baseline model. However this model still have problem with the context loss and feature dilution. In this paper, we propose a new model to address this problem of UNet model by utilizing one of the latest attention module named Coordinate attention (Hou et al., 2021).

Along side the development of baseline model, attention modules have also been proved to achieve high results in brain tumor segmentation including Multi-scale guided attention (Sinha and Dolz, 2019), Cross-task Guided Attention (Zhou et al., 2019) and Attention UNet (Oktay et al., 2018). Furthermore, many attention modules have been proved very effective in segmentation task such as Squeeze-and-

Excitation (Hu et al., 2017) and Coordinate attention (Hou et al., 2021). Even though these attentions have high results in segmenting normal image. Their method is not suitable to work with MRI scans which have high variance. We also propose a modification of coordinate attention to cope with the MRI scans.

In order to demonstrate the effective of our designed. We did experiments on the BraTS 2020 dataset (Menze et al., 2015) with the origin UNet model and our proposal. The results show the improvement of our proposal in both model design and attention module design.

2 RELATED WORK

In this section, we present a brief overview of recent method to handle the context problem of UNet model and attention module design.

2.1 UNet Model Improvement

Many work have tried to solve the context problem of UNet model. Attention U-Net (Oktay et al., 2018) applied attention gate to enhance the skip connection features. UNet++ (Zhou et al., 2018) redesigned the skip connections to reduce the gap between contracting path and expanding path. UNet 3+ (Huang et al., 2020) applied the full-scale skip connection to incorporate low-level details with high-level semantics from feature maps in different scales. DC-UNet (Lou et al., 2021) proposed the dual channel block to replace the traditional convolution blocks.

2.2 Attention Modules

Attention have been proved effective in brain tumor segment task. Using attention gate to filter the skip connection in Attention UNet (Oktay et al., 2018), applying attention at multi-scale feature in Multi-scale guided attention (Sinha and Dolz, 2019), Cross-task Guided Attention (Zhou et al., 2019) developed a specific module to work with multi tasking model. Squeeze-and-Excitation Network (Hu et al., 2017) proposed a attention module to captured the channel-wise relationship. Inspired by the Squeeze-and-Excitation Network, coordinate attention (Hou et al., 2021) further encoding coordinate info along with channel-wise relationship.

3 METHOD

In this section, we propose the design of UNet model with attention module in the first part. In the second part, we propose a modification of the Coordinate Attention module (Hou et al., 2021) to be more suitable with MRI scans data.

3.1 Coordinate Attention UNet

In 2015, UNet model (Ronneberger et al., 2015) is proposed, which achieved the highest ranking in ISBI cell tracking challenge in the same year. The model is divided into two parts. A contracting path to capture context and a symmetric expanding path that enables precise localization.

Both paths are comprised of multiple convolution layers followed by sampling operations. The contracting path executed downsampling, which reducing the size of image. On the contrary, the expanding path used upsampling to expanded the encoded features causing the feature dilution. To further enhance the context for upsampling operations, UNet model added skip connections between contracting path and expanding path to use the context from the contracting to enhance the diluted features.

Downsampling step is done by applying 2×2 max pooling. Figure 1 show a sample result of this operation. As we can see, the size of the input is reduced by half, which meant half of the feature is lost after downsampling. In other to utilize the lost features, we applied coordinate attention to the feature map before passing it to the downsampling. This result in the design of the left side of our model showed in Figure 3.

Upsampling is done by applying transposed convolution with kernel size 2×2 and stride 2. Fig-

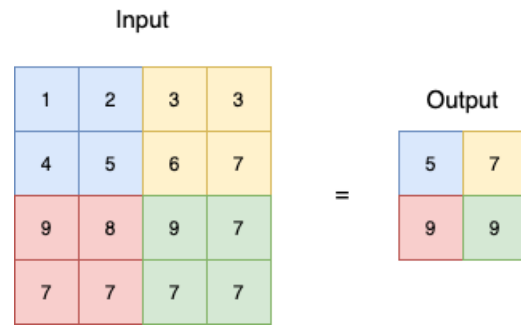


Figure 1: Max pooling operation sample with kernel 2×2 and stride 2.

ure 2 demonstrate a sample result of this operation. As we can see, the encoded features are expanded by two times. By applying coordinate attention to the expanded segment map, we augmented it with direction-aware and position-sensitive attention maps. We demonstrated this design in the right side of Figure 3.

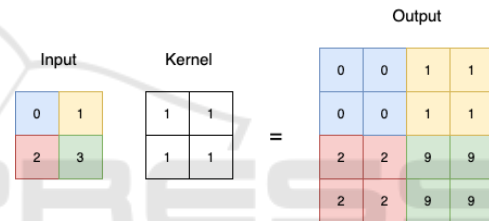


Figure 2: Transposed convolution of input size 2×2 and kernel size 2×2 .

3.2 Coordinate Attention for MRI Scan

Coordinate attention module (Hou et al., 2021) can be divided into two part. The first part is called coordinate information embedding and the second part is coordinate information generation. In this work we modified the the first part of the module.

Developed from Squeeze-and-Excitation attention (Hu et al., 2017), Coordinate Attention (Hou et al., 2021) have added the ability to encode coordinate attention by applying average pooling for along horizontal coordinate and vertical coordinate. Given the input X , the output of the c -th channel at width w is formulated as:

$$z_c^w = \frac{1}{H} \sum_{0 \leq j < H} x_c(j, w) \quad (1)$$

And the output of the c -th channel at height h is formulated as:

$$z_c^h = \frac{1}{W} \sum_{0 \leq i < W} x_c(h, i) \quad (2)$$

While this method have been proven effective, it is not suitable to use average pooling for data high

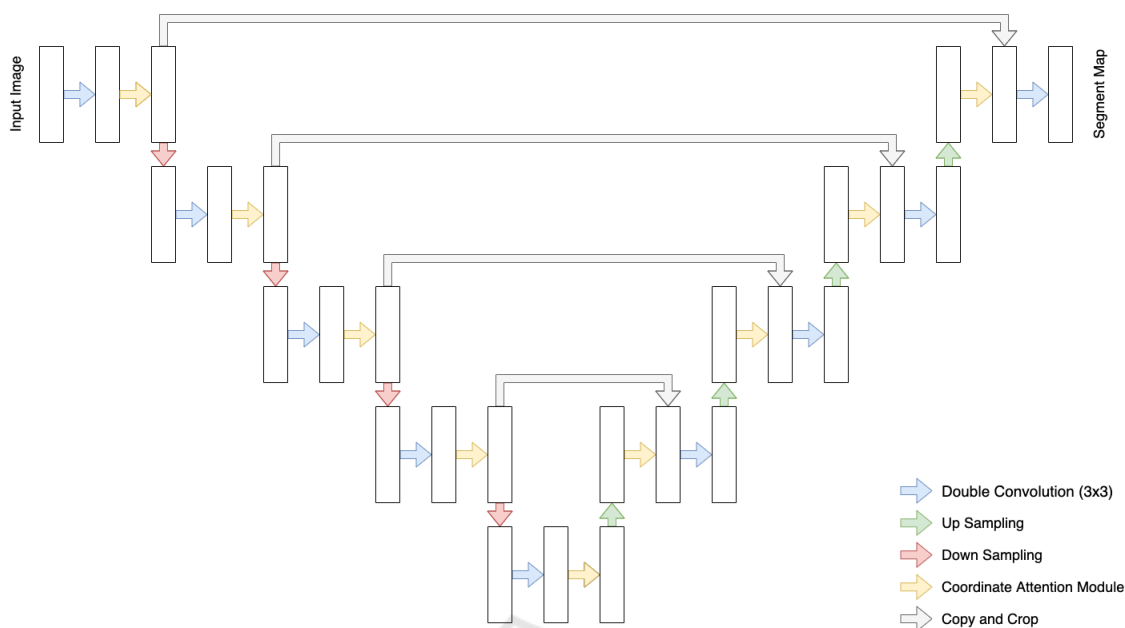


Figure 3: Coordinate Attention UNet architecture.

variance (Boureau et al., 2010) such as MRI scans. Therefore we changed the pooling function to max pooling. The c -th channel output at width w become:

$$z_c^w = \max_{0 \leq j < H} x_c(j, w) \quad (3)$$

And the output of the c -th channel at height h is formulated as:

$$z_c^h = \max_{0 \leq i < W} x_c(h, i) \quad (4)$$

Then the encoded features is then passed through attention generation part to generate two attention features. These features is used to re-weight the input features.

4 EXPERIMENT

In this section, we describe the dataset we use to evaluate our models. Next we explain how we setup the experiments and evaluate the output. Finally we show the comparison result of our model.

4.1 BraTS Dataset

In our experiment, we use BraTS 2020 dataset (Menze et al., 2015) for training our model. This dataset is used for holding 2020 BraTS Challenge (Bakas et al., 2018), which is the most famous challenge in Brain Tumor segmentation task. The data

provided is collected from real patients and labeling by specialist.

The data is provided as a 3D image in nifty format. One image contains 155 layers of 240×240 images. Further more, the intensity value of images is not in the range of 0-255 like normal images, which make the data more special to handle.

Data of a single patients includes four modalities of MRI scans, native image (T1), a post-contrast T1-weighted (T1Gd), T2-weighted (T2), and T2 Fluid Attenuated Inversion Recovery (T2-FLAIR). Figure 4 show a sample of each image types.

The dataset have three segment labels, the GD-enhancing tumor (ET — label 4), the peritumoral edema (ED — label 2), and the necrotic and non-enhancing tumor core (NCR/NET — label 1).

4.2 Experiment Setup

In order to evaluate our work, we implement three models: original UNet model, Coordinate Attention UNet model (CA-UNet), Max pooling Coordinate Attention UNet model (MCA-UNet).

All model is implemented using PyTorch (Paszke et al., 2019). We use Adam Optimizer with the learning rate 1×10^{-5} . Model is trained using the batch size of 5 in 5 epochs. As the attention module is harder to converge, we first train the UNet model then used the pretrained weight to training CA-UNet and MCA-UNet. The result is calculated using Segmentation Metrics Library (Jia, 2020).

Table 1: Experiment results. The result is calculated based on new training data in BRATS2020 dataset.

Model	Dice Score			Hausdorff95		
	ET	TC	WT	ET	TC	WT
UNet	0.82585	0.84112	0.91564	2.68228	7.98642	7.48138
CAUNet	0.80907	0.83106	0.91346	5.90530	8.29032	7.86522
MCAUNet	0.82006	0.84607	0.91898	5.44802	7.55089	7.26619

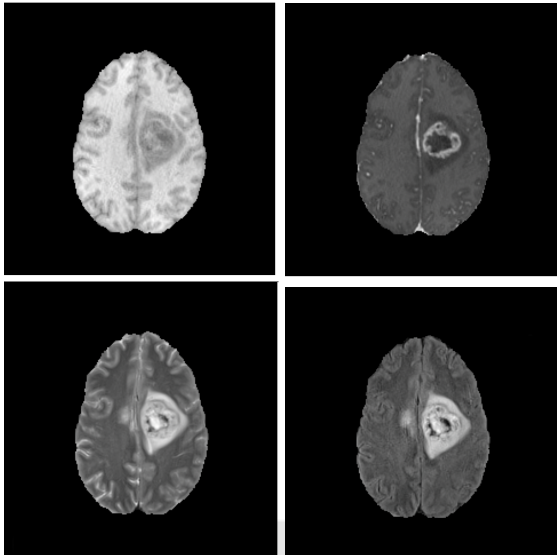


Figure 4: Four modalities of an MRI scan layer. On the first row is T1 Image and T1ce Image. The second row contain T2 Image and Flair Image.

4.3 Model Comparison

We can qualitatively compare the difference between each model in Figure 5. As we can see MCA-UNet and CA-UNet have better segment for necrotic and non-enhancing tumor core (NCR/NET) and. Furthermore MCA-UNet's segmentation of NCR/NET have better structure than CA-UNet.

For more detail comparing our model, we calculate Dice Score, and 95 percentile Hausdorff Distance for three segment target: Whole Tumor (WT), Tumor Core (TC) and Enhance Tumor (ET). Table 1 record result of both score.

As we can see, UNet still shine above all model in segmenting Enhance Tumor. But in the rest targets, MCA-UNet scored higher than the original UNet. Furthermore, CA-UNet scored lowest among them. But with the modification in MCA-UNet, the scored improved significantly, which proved the effectiveness of our proposal.

5 DISCUSSION AND CONCLUSION

In this section, We describe what we haven't done in this article and how we can improve the performance of our work. The first topic is Data Augmentation, the second topic is moving to 3D model

5.1 Data Augmentation

Data imbalance and intensity normalization are two biggest issue MRI scans. In this section we discuss and how to handle those two issue and also how we made used of the four modalities of one MRI scans.

As we can see in Figure 5. The tumor region is only cover around 10% of the whole image and around 30% of the brain, which cause the imbalance between segment mask and the image. To handle this issue, we can crop the image to make the brain and segment mask cover more percent of the image. In our work, we did not cropped the images because we want to evaluate the model efficient without data augmentation.

To handle data normalization, an effective method is applying N4 Bias Correction (Tustison et al., 2010). The N4 bias field correction is a famous algorithm to handle the low frequency bias in MRI scans which make the intensity become uniform. In future work, we can apply this algorithm to do more experiment.

MRI scans is a 3D data which is not fitted for our model. Therefore we decided to slice each layer of the MRI scans and used it as the input of our model. This method prevent us from using the relationship of z-axis feature of each image. Instead of the z-axis relationship, we make use of four modalities of the image by compressing four modalities in to one 2D image with four channels. To make use of this setup is one of the reason why we chose the coordinate attention module which have ability to enhancing channel-wise relationships.

5.2 Moving to 3D

As we mentioned in section 5.1, our work focus on 2D model. This method removed the z-axis relation-

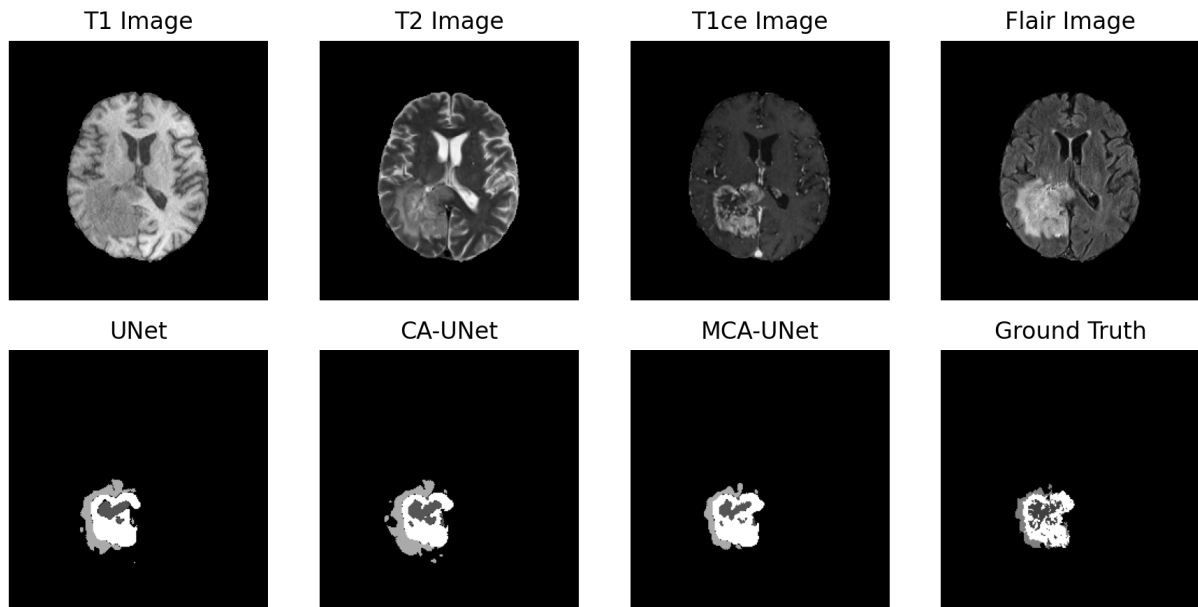


Figure 5: Segmentation result of three models. The first row is the four image types of the input image. The second row show the prediction of UNet, Coordinate Attention UNet (CA-UNet), Max pooling Coordinate Attention UNet (MCA-UNet) and Ground Truth. GD-enhancing tumor (ET) is colored white, the peritumoral edema (ED) is colored light grey, and the necrotic and non-enhancing tumor core (NCR/NET) is colored dark grey.

ship, which is an important feature of 3D data. Therefore in the futures, we can continue our research with applying attention to 3D model to encode the z-axis relationship.

In this research, we also found that compressing all modalities into one image have positive affect on the results of our model. In the future work, we can exploring the effectiveness of this method with 3D data.

5.3 Conclusion

In this paper, we proposed a new UNet model, which utilize the attention mechanism to solve the context loss and feature dilution of original UNet. We also proposed a modification of Coordinate Attention Module to be more suitable with the MRI scans data. These proposal have been proved effective with our experiments.

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