

# Random-walk Segmentation of Nuclei in Fluorescence Microscopic Images with Automatic Seed Detection

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**Abstract:** In personalized immunotherapy against cancer analysis of cell nuclei in tissue samples can provide helpful information to predict whether the benefits of the therapy outweigh the usually severe side effects. Since segmentation of nuclei is the basis for all further analyses of cell images, research into suitable methods is of particular relevance. In this paper we present and evaluate two versions of a segmentation pipeline based on the established random-walk method. These versions contain automatic seed detection, using a distance transformation in one of them. In addition, we present a method to select the required hyper-parameter of the random-walk algorithm. The evaluation using a benchmark dataset shows that promising results can be achieved with respect to common evaluation metrics. Furthermore, the segmentation accuracy can compete with a reference *CellProfiler* segmentation pipeline, based on the watershed transformation. Based on the presented pipeline, the random-walk method can also be integrated into more advanced pipelines to further improve segmentation results.

## 1 INTRODUCTION

With 10 million deaths caused by cancer in 2020, it is one of the most common causes of death worldwide (World Health Organization, 2021). In the fight against cancer, immunotherapy has become a promising treatment option by using the body's immune system to fight cancer (Esfahani et al., 2020). The discovery of immune checkpoint inhibitors, which prevent tumor cells from using immune escape mechanisms, was of great importance for research.

There is still insufficient research into which people benefit from this kind of treatment. A preselection is particularly important because the side effects can be severe and even fatal (Esfahani et al., 2020). As part of the *ImmunePredict* research project, we aim at improving this selection by developing a predictive model based on fluorescence microscopy imaging. The first step in analyzing the images is to segment nuclei to accumulate cellular information for predicting treatment success in further steps.

For segmentation, different methods were proposed, that can be divided into the categories of optimization, threshold and machine-learning-based methods (Abdolhoseini et al., 2019). The latter is usually considered state-of-the-art and produce promising results for nuclei segmentation (cf. Liu et al., 2021; Zaki et al., 2020; Kowal et al., 2020). Neverthe-

less, segmentation of nuclei remains challenging. For example, overlapping nuclei are typically segmented less accurately. A common approach is to use hybrid methods by combining multiple techniques. The watershed transformation, which was evaluated as a part of our research project (Wirth et al., 2020), for example, can be combined with threshold and model-based methods (Abdolhoseini et al., 2019) or used for post-processing (Kowal et al., 2020), to improve segmentation of clustered cell nuclei.

The random-walk algorithm can be widely applied for image processing (e.g. image fusion, registration and segmentation) and it has already been applied successfully for segmentation in the oncological field (Wang et al., 2019). Besides the model we use in this paper, proposed by Grady (2006), there are alternating models to suit different use cases (Wang et al., 2019). Key points in the improvement of the algorithm are the preprocessing of input data and the position of required seeds, that typically need user interaction (Wang et al., 2017). An automatic solution is necessary to make better use of the algorithm and to combine it with e.g. deep learning methods.

The aim of this paper is to explore the basic potential of the random-walk method for segmentation of nuclei in fluorescence images by assessing the performance of two pipeline versions we developed. We follow an automatic approach by proposing two au-

tomatic seed detection methods with appropriate pre-processing for detection and the random-walk algorithm itself, as well as a method to set the hyperparameter  $\beta$  (see (1)). This enables the use of our pipeline separately or in combination with sophisticated techniques.

This paper is organized as follows: We summarize the concept of segmentation using the random-walk method in section 2. After that we outline the implementation of our pipeline in section 3, which we evaluate using a publicly available dataset presented in section 4 and the metrics listed in section 5. The results are presented in section 6 followed by the discussion in section 7. We provide a summary of our findings and concluding remarks in section 8.

## 2 RANDOM-WALK SEGMENTATION

A random-walk is a stochastic process that can be used to describe random movements (Grady, 2006). For segmentation, the random-walk is considered in at least two dimensions. It operates on an undirected graph and has a bias, which means that the steps on this graph have different probabilities represented as edge weights (Grady, 2006).

The segmentation method used in this paper was proposed by Grady (2006). Grady (2006) derived a method for analytically computing the desired probabilities without the need of a rather inefficient simulation of a random-walk. The result of this method is an image that is segmented into regions that are assigned their own specific label. It is necessary to assign labels to certain pixels (seeds) in advance. The remaining pixels are assigned to these labels using the random-walk algorithm by calculating the probability that a random-walker that starts at a pixel will first reach a seed with a certain label (Grady, 2006).

The algorithm is based on the conversion of the image into a graph  $G = (V, E)$  that consists of nodes  $v \in V$  and edges  $e \in E$ . To prevent the random-walker from crossing sharp intensity gradients, the edges are weighted with a weighting function. As described in (Wang et al., 2019) different weighting functions have been proposed. We use the Gaussian weighting function (see (1)) in our pipeline:

$$w(e_{i,j}) = w_{i,j} = e^{-\beta(g_i - g_j)^2} \quad (1)$$

The edge  $e_{i,j}$  connects the neighboring nodes  $i$  and  $j$ .  $\beta$  is the only free parameter in the algorithm. The intensities of the pixels are denoted as  $g_i$  and  $g_j$ . The probability with which the random-walker uses

an edge is referred to as  $w(e_{i,j})$ . Thus, strong intensity gradients yield small probabilities.

The required probabilities are determined by solving a sparse linear system of equations. For each node a  $k$ -tuple vector  $x_i = (x_i^1, \dots, x_i^k)$  is computed. The final segmentation is determined by assigning each node  $v_i$  to the label corresponding to  $\text{argmax}(x_i^s)$ .

The algorithm always comes up with the same unique result, which depends on the seed selection. For completely black images or noise, the method creates a so-called neutral segmentation. For each seed, the segmented areas then resemble Voronoi cells (Grady, 2006).

## 3 IMPLEMENTATION

Our proposed pipeline are based on methods of the following standard python libraries: *NumPy*<sup>1</sup>, *SciPy*<sup>2</sup>, *OpenCV*<sup>3</sup>, *scikit-image*<sup>4</sup> and *pandas*<sup>5</sup>. Figure 1 shows a schematic representation of our pipeline.

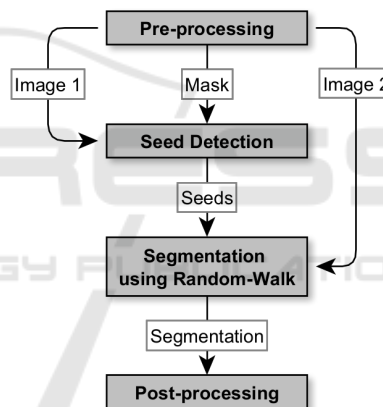


Figure 1: Schematic representation of the pipeline for segmentation using the random-walk algorithm.

An image is taken from a dataset and pre-processed. Since a distance transformation is optional in the preprocessing step, there are two versions of the pipeline, which, however, do not differ in the general process. Preprocessing produces one image that is used in seed detection and a second one that is used for segmentation. In addition a mask seed detection is created. As the first preprocessing step we reduce noise in all of three images with the non-local-means method, the contrast is optimized with the help of an adaptive histogram equalization and edges are en-

<sup>1</sup><https://numpy.org/> (version 1.18.5)

<sup>2</sup><https://www.scipy.org/> (version 1.5.0)

<sup>3</sup><https://opencv.org/> (version 4.5.1.48)

<sup>4</sup><https://scikit-image.org/> (version 0.16.2)

<sup>5</sup><https://pandas.pydata.org/> (version 1.0.5)

hanced by using a Sobel filter.

To create the mask we use the Li threshold (Li and Lee, 1993) after that and then filter out small objects to prevent detection of seeds for artifacts in the background. If the distance transformation is to be used before seed detection, we apply the Li threshold on an image with 1.5 times more enhanced edges, only using strong edges. After the transformation, a Gaussian filter is applied and the intensity values get stretched to cover values from 0 to 255. Without the transformation, only the last two steps are required after the edge enhancement.

The image, to which the random-walk algorithm is applied, demands a different preprocessing. Hence, we use a background subtraction after noise reduction and stretch the intensity values as described before. Lastly, we dim intensity values to 40% of the maximum intensity to reduce contrast in bright regions.

In the developed pipeline, local maxima are used as seeds. In order to avoid too many seeds per object and yet not set an overall upper limit, only seeds that are at least ten pixels apart are accepted. The determined seeds are marked in a labeled image. In addition, the biggest region of the background, after dilating the objects in the mask from preprocessing, is marked as a background seed. If a distance transformation is used, the seeds for the nuclei are dilated before labeling.

Using the *random\_walker()*-method of the *scikit-image* library, a segmentation of the image is created. As post-processing, objects that are larger than a pre-defined value (here 5000) are removed from the image and the biggest object is labeled as the background.

## 4 DATASET

The image dataset BBBC039v1<sup>6</sup> (Caicedo et al., 2019), available from the Broad Bioimage Benchmark Collection (Ljosa et al., 2012), was used for evaluating the two pipeline versions. The collection was published by the Carpenter lab at the Broad Institute and contains sets of microscopic images. In addition, the sets contain a ground truth for each image as well as metadata.

The metadata describes a division into training, validation and test set consisted of 100, 50 and 50 images respectively. For this paper, these sets were used as follows: The training dataset was used during pipeline development. The validation dataset was used to determine the  $\beta$  parameter. Finally, the test dataset is used to evaluate the segmentation accuracy.

<sup>6</sup><https://sites.broadinstitute.org/bbbc/BBBC039>

### 4.1 Image Data

The BBBC039v1 image set contains 200 images in which nuclei of cell line U2OS can be seen. The human osteosarcoma cell line U2OS was obtained from a tumor in the tibia of a 15-year-old girl in 1964 (Niforou et al., 2008). The images were acquired with a fluorescence microscopy where the DNA was stained with Hoechst. They have a resolution of  $520 \times 696$  pixels and are stored as 16-bit TIFF files.

This dataset is rather challenging because of strong intensity differences within and between the nuclei. Some of them overlap or touch each other. The size and shape of nuclei can differ due to a wide variety of phenotypes, including micronuclei, toroidal, fragmented, round and elongated nuclei (Caicedo et al., 2019). The number of nuclei in an image varies between 0 and 231. All images contain some noise and a couple of images are almost entirely filled with noise. In addition, some images contain bright artifacts that cover up nuclei or cause strongly reduced intensity values in surrounding areas. A total of approximately 23000 nuclei were manually segmented by biologists for this dataset.

### 4.2 CellProfiler Pipeline

The Broad Institute has also published a reference pipeline for the *CellProfiler*<sup>7</sup> software, which is a possible solution to the segmentation problem.

The preprocessing steps of this pipeline include morphological operations, background subtraction and applying a Sobel filter to enhance edges. A Gaussian filter is applied to the image and a binary image is created using a global Li threshold (Li and Lee, 1993). Even though the typical diameter is specified with 20 to 80 pixels, objects outside these limits are not discarded. Then, objects are identified that potentially contain multiple nuclei. For these objects a distance transformation is applied and the local maxima of its output are used as seeds for a watershed transformation. All maxima that are less than ten pixels apart are discarded. A smoothing filter is used to post-process the segmentation to prevent over-segmentation. Finally, all holes in the objects are filled.

## 5 EVALUATION METRICS

Despite the importance of evaluating a segmentation algorithm, there is no consensus on how it should be

<sup>7</sup><https://cellprofiler.org/>

done (Sonka et al., 2015). As part of the *ImmunePredict* project, suitable evaluation metrics for supervised evaluation were selected (Wirth et al., 2020). They include pixel- and object-based methods. The ground truth data in the BBBC039v1 dataset are used as reference ( $R$ ) for the created segmentations ( $S$ ).

## 5.1 Pixel-based Metrics

Pixel-based evaluation can be obtained through calculation of the Rand Index (RI) (Rand, 1971) and the Jaccard Index (JI) (Jaccard, 1901). They consider whether pixels of pairs of pixel in  $R$  or  $S$  are assigned to the same or to different objects. The intensities in  $S$  are called  $S_i$  and  $S_j$  and  $R_i$  and  $R_j$  in  $R$ . All combinations of pixels are considered as long as  $i \neq j$ . The pairs are divided into the groups  $A$  to  $D$  according to following scheme.

$$\begin{aligned} A: S_i = S_j \wedge R_i = R_j & \quad C: S_i = S_j \wedge R_i \neq R_j \\ B: S_i \neq S_j \wedge R_i = R_j & \quad D: S_i \neq S_j \wedge R_i \neq R_j \end{aligned}$$

Groups  $A$  and  $D$  contain pixel pairs for which  $S$  and  $R$  agree that pixels of the pair belong to the same object or not. Conversely, groups  $B$  and  $C$  contain the pairs for which there is no agreement in this respect. The number of pairs in the corresponding groups are denoted by  $a$ ,  $b$ ,  $c$  and  $d$ . Thus the RI is given by:

$$RI(R, S) = \frac{a + d}{a + b + c + d} = \frac{a + d}{\binom{n}{2}}. \quad (2)$$

Here  $n$  denotes the total number of pixels in  $S$  and  $R$  respectively. If  $S$  and  $R$  overlap completely, the index takes a value of 1. If there is less overlap, the value is lower.

The above definition of  $a$ ,  $b$ ,  $c$  and  $d$  is also used to calculate the JI:

$$JI(R, S) = \frac{a + d}{b + c + d}. \quad (3)$$

The upper limit for JI depends on the number and size of nuclei in relation to the image size. Thus, it only allows a comparison between segmentations that were created for the same data.

## 5.2 Object-based Metrics

For object-based metrics, reference objects in  $R$  must be assigned to the objects in  $S$ . The object in  $R$  is determined with which an object in  $S$  shares the most pixels. On this basis, the maximum of the smallest distance between two objects can be calculated, which is called the Hausdorff Distance (HD). This can be calculated as described by Coelho et al. (2009).

$$HD(R, S) = \max D(i) : S_i \neq R_i \quad (4)$$

Where  $D_i$  is the minimum distance of a pixel  $i$  on the object boundary to a pixel on the boundary of the reference object. The mean value of all Hausdorff Distances is used to evaluate an entire image.

Using  $D_i$ , the Normalized Sum of Distances (NSD) for each object can also be calculated as described by Coelho et al. (2009) as follows.

$$NSD(R, S) = \frac{\sum_i [R_i \neq S_i] * D(i)}{\sum_i D_i} \quad (5)$$

The index  $i$  iterates over all pixels of the union of both objects. As for the HD, the mean value of all distances in the image is calculated for the NSD of the whole image.

The Error Counting Metrics (ECM) also belong to the object-based evaluation methods and count Missing, Added, Merged and Split objects. They thereby quantify errors that are intuitively identified by human observers (Coelho et al., 2009). For the calculation of the ECM, a list of assignments of objects in  $S$  to objects in  $R$  is used and additionally a list of reverse assignments. Here, the background in  $S$  and  $R$  represents a separate object. An assignment only happens if the number of common pixels is greater than half the number of pixels of the object for which an assignment is sought. Objects that are significantly larger in  $S$  than in  $R$  can thus be interpreted as Added and those that are significantly larger in  $R$  as Missing. The four metrics are defined as follows:

- Split: Number of objects in  $R$  assigned to more than one object in  $S$ .
- Merged: Number of objects in  $S$  assigned to more than one object in  $R$ .
- Added: Number of objects in  $S$  assigned to the background in  $R$ .
- Missing: Number of objects in  $R$  assigned to the background in  $S$ .

For the BBBC039v1 dataset, an alternative calculation of the assignments was also proposed, where the intersection-over-union is calculated and the assignments are determined using a threshold (Caicedo et al., 2019). In comparison the second method marks objects that are marked as Added as Missing too. This results in a substantially increased number of Missing-errors. This is why the previously described calculation is used in this work; besides, it is also used in the *ImmunePredict* project before (Wirth et al., 2020).

## 6 RESULTS

Following results were produced using the dataset described in section 4. In order to quantify the segmentation success, the evaluation metrics presented in section 5 are used. In section 3 two pipeline versions were presented. In order to improve readability, the version without distance transformation will be referred to as 'version 1' and the one with as 'version 2'.

### 6.1 Selection of the $\beta$ Parameter

The parameter  $\beta$  (see (1)) plays a crucial role in the segmentation process. Based on the metrics presented in section 5 the ratio of pixel- to object-based metrics (6) is presented as a decision criterion for selection of  $\beta$ .

$$Ratio = 10 * \frac{JI + RI}{HD + NSD + \sum ECM} \quad (6)$$

The selection is done by using the validation hold-out set. Figure 2 shows the average results of version 2 for different  $\beta$  values. The results of version 1 are very similar, so that the same beta value was selected. The  $\beta$  values to consider lie within the range of 10 to 200 with equidistant spacing.

The RI and JI initially rise sharply with an increase in the  $\beta$  value and then decline slightly but steadily, starting from a value of around 50. The largest average HD is measured for the smallest  $\beta$  value. After which the value drops sharply. Then it rises slightly, but falls roughly from a  $\beta$  value of 90. The NSD values behave similarly to the HD values for low  $\beta$  values. As the values increase, NSD remains low for longer and then increase slightly.

The ECM show different trajectories. The average number of Split-errors is consistently lowest and almost remains at the same level. The number of Added-errors is just above this, whereby a falling trend can be observed up to a  $\beta$  value of 100. For the Merged-error the numbers decrease slightly with the increase of  $\beta$  and are more than twice as high as for the Added-error most of the time. The Missing-error is the most frequent error for both versions. Its average number decreases up to a  $\beta$  value of 50 and then increases with higher values.

The course of the ratio between pixel- and object-based metrics emerges from the described courses for the evaluation metrics. For version 1, these values are consistently lower than those for version 2 because the latter achieves mostly higher values for pixel-based and mostly lower values for object-based metrics. The optimal value for  $\beta$  corresponds to the maximum of the mentioned ratio. For a comparison

of the two versions with the *CellProfiler* pipeline (CP version) the value for  $\beta$  gets fixed to 50.

### 6.2 Pipeline Comparison

Table 1 compares the average results of the version 1, version 2 and CP version. The values of the pixel-based metrics are similar for all versions. The CP version has the lowest RI, but a higher JI. Both the HD and NSD are lowest for version 2, whereby version 1 and 2 achieve similar values for these metrics.

Differences between our proposed versions are noticeable for the ECM. Except for the number of Split-errors, the values of version 2 are lower than those of version 1. The CP version causes fewer Missing-errors compared to the other two versions, but more than three times as many Added-errors. The number of Merged- and Split-errors is also highest for the CP version. Despite fewer Missing-errors, the sum of all ECM for the CP version is the highest.

This is also reflected in the lower ratio value for the CP version. Version 2 achieves the best metric scores most of the time, what results in the highest ratio.

Figure 3 shows example results on the test dataset for version 1, version 2 and CP version in comparison to the ground truth. Segmented nuclei are colored randomly to facilitate the differentiation of touching cells. In general, the results for the ECM can be detected. In the segmentations of the CP version, for example, more Merged-errors can be recognized. Compared to the ground truth, the missing nuclei can also be identified, which are the cause of the high Missing-error values mentioned.

## 7 DISCUSSION

As described in section 4, the ground truth used for evaluation is a manual segmentation. Therefore, the dataset may be affected by intra- and inter-observer-variability. We will not analyze these effects further.

The effect of the  $\beta$  parameter (see (1)) on the resulting segmentation causes the trajectories in Figure 2. For higher values, smaller weights between neighboring nodes result in small objects, which leads to increase in NSD, decrease in RI and JI but less Merged-errors. In return, there might be more Missing-errors. Smaller  $\beta$  values mean higher weights between nodes and a significant increase in object size, resulting in a high HD and number of Added-errors. A suitable choice of parameter balances these effects. During the development of the pipeline,  $\beta$  was set to 130 (default value of *scikit-image*-method). The selection of the

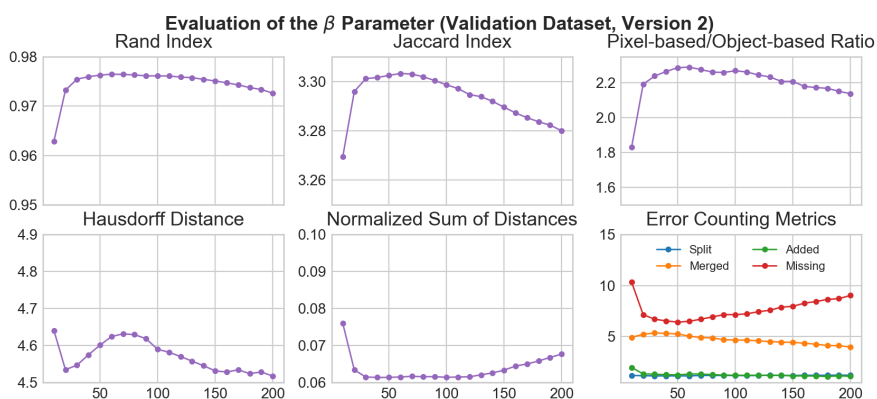


Figure 2: Average results of version 2 on the validation dataset for Rand and Jaccard Index, Hausdorff Distance, Normalized Sum Of Distances, Error Counting Metrics and the ratio between pixel- and object-based metrics for  $\beta$  values from 10 to 200.

Table 1: Results of pipeline version 1 and 2 ( $\beta=50$ ) and the *CellProfiler* pipeline on test dataset. Results are the average values of the Rand and Jaccard Index, Hausdorff Distance, Normalized Sum Of Distances and Error Counting Metrics (Split, Merged, Added, Missing) as well as the ratio between pixel- and object-based metrics. Best results are marked in gray.

Version	Pixel-based		Object-based				Ratio		
	RI	JI	HD	NSD	Split	Merged		Added	Missing
1	0.9778	4.1928	4.7973	0.0684	0.7000	5.7600	1.4400	6.3000	2.7120
2	0.9788	4.1947	4.6611	0.0645	1.1000	5.3200	1.4000	5.7400	2.8293
CP	0.9701	4.2115	5.1847	0.0946	1.3400	6.8600	5.0200	4.3800	2.2648

parameter could be done automatically by determining the maximum of the ratio of pixel- to object-based metrics. This leads to  $\beta = 50$  for the dataset used. As can be seen in table 1, the fixed value turns out to be a suitable setting for the whole test set on the average. The values for pixel-based metrics differ only slightly between the compared versions. In contrast, the object-based metrics clearly indicate that our proposed pipeline achieves superior performance. This is also confirmed by the overall higher ratio values. Before using the segmentation pipeline on a new dataset, especially with images from other modalities, it will still be necessary to redefine the  $\beta$  value and potentially adjust the preprocessing.

Also other segmentation pipelines were evaluated on the BBBC039v1 dataset. Compared to deep learning methods as presented in Caicedo et al. (2018), the proposed pipeline perform a little worse in terms of Merged- and Split-error. Missing-errors are again lower for our pipeline, but this may also be due to the different calculation of the JI. Liu et al. (2021) have also evaluated several deep learning methods using this dataset. Their evaluation metrics differ from those in this paper, which makes a direct comparison difficult.

The results of the random-walk algorithm significantly depend on the seed placement. For optimal segmentation, one seed must be set at a suitable location for each nucleus. Because expert knowledge

to set seeds involves a great deal of effort we proposed an automatic approach, described in section 3. Approaches for automatic seed determination for random walk have already been explored for specific problems, such as tumor or liver segmentation, and different modalities (e.g. 3D CT, 3D MRI) (Wang et al., 2019). Intensity values of pixels are often used for seed determination.

We use intensity values to distinguish nuclei from the background in fluorescence microscopy images. Due to a combination of thresholds and local maxima, appropriate seeds can be selected. By using the distance transformation, additional information about the shape of the objects is included. From the results shown in table 1 it can be concluded that the proposed seed detection methods are suitable for this setting. Since the two proposed versions differ only in the use of a distance transformation before seed detection, it can be concluded that such a transformation improves seed detection in cell nuclei images. Yet, it should be noted that it causes more Split-errors. This type of error occurs more often for nuclei that have an elongated shape and are notched in the middle. For the present dataset, this effect occurs only sporadically. When using the pipeline with other data or methods, the detection method should then be selected according to the prevailing nuclei shapes.

For some images in the dataset segmentation is particularly challenging. One example are images

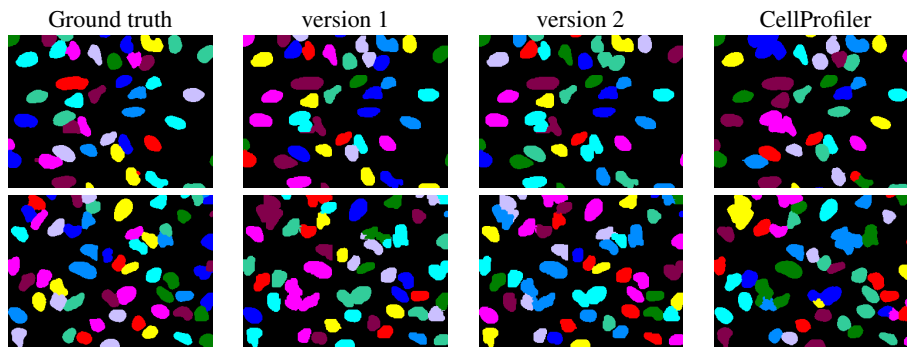


Figure 3: Example results for version 1, version 2 and CP version using images of the BBBC039v1 dataset compared with the ground truth. Cropped images are shown in which the objects are randomly coloured.

that are highly noisy or show artifacts. For the former, the ground truth for this image is empty and shows no nuclei. Therefore results for such images are not included in the evaluation because neither the calculation of the HD nor the NSD would be possible, as reference objects are needed for the calculations of both metrics. This affects two images in training set and one image in validation set.

Due to different phenotypes, the sizes of the nuclei can vary greatly. In order not to determine seeds for artifacts in the image, small objects are filtered out as described in section 3. The downside of this approach is that no seeds are determined for a large part of the micronuclei. These nuclei are either segmented as part of the background or merged with nuclei in the neighborhood. The hole inside toroidal nuclei can also be a challenge for segmentation method because a strong intensity gradient exists between the hole and the rest of the nucleus. Due to the random-walk algorithm's property of creating only smooth segmentations, the pipeline is robust to these morphologies as long as only one seed is set per nuclei.

Additionally, the shapes created by touching nuclei can influence the segmentation. Smaller nuclei can form structures that resemble shapes of larger nuclei. After a distance transformation, no adequate number of seeds can be found because only the nuclei that have the greatest distance to the background receive a seed, resulting in more Merged- and Missing-errors. If the contrast is very low, even cutting out the transformation only improves the results slightly. The same effect on ECM applies to images with strong artifacts, which cause a strongly reduced contrast in both bright and dark areas. In addition, the number of Added-errors is higher because some objects are significantly larger than in the ground truth.

The runtime of methods based on the random-walk is known to depend on the speed with which the linear system of equations can be solved (Wang et al., 2019). Our background seed detection can save

runtime because many background pixels are already labeled. Since the number of these pixels varies, the variance of the running time per image remains high. This yields in a runtime of around 3 minutes (64 Bit Windows, i5-10400 2.90GHz, 16GB RAM) for the whole test dataset.

Throughout the pipeline, different values (e.g. maximum object size and minimum distance of seeds) must be set. These values should be selected according to the available metadata. Since different magnifications can be used for microscopy images, a calculation, e.g. based on the resolution, is not useful.

## 8 CONCLUSION

In the context of this paper, two versions of a pipeline were developed which use the random-walk algorithm to segment nuclei. The versions differ in their seed detection, as the second version uses a distance transformation. We propose a way of determining the free parameter of the random walk automatically by using the ratio of the evaluation metrics.

For a benchmark dataset with fluorescence microscopy images, both versions achieve good results with respect to different evaluation metrics. These results and the comparison with the CP pipeline show that the developed pipeline is suitable for segmenting fluorescence microscopy images of nuclei. Especially for object-based evaluation metrics, the two developed versions consistently reliably achieve good values. The pipeline is robust against different morphologies of the cell nuclei. However, micronuclei are often missing in the segmentation results because corresponding seeds are not generated.

Many typical challenges of a medical context are included in the dataset used. This allows an evaluation of the pipeline in terms of its use in such a setting. The heterogeneity of the image data poses a challenge

for segmentation algorithms and seed detection. The latter has a great influence on the quality of the segmentation. The use of local maxima as seeds and the developed method to determine a background seed is suitable for the present dataset. The results can be further improved by a preceding distance transformation, but results in more Split-errors. However, further evaluations on other data sets are needed to make a more general statement on performance.

Following aspects can also be content of further research: An extension of the range of intensity values when handling the images to use the full 16 bits of the TIFF images instead of 8 bits. Improving the runtime by using further preprocessing or other solvers for the system of equations. It is also interesting to explore how the pipeline can be used for 3D data.

The results of this paper can further serve as a basis for an integration of the random-walk algorithm in more sophisticated pipelines based on deep learning (e.g. as post-processing). We are planning further evaluation and testing of this kind of integration. In addition, the developed pipeline is suitable to provide reference benchmark results for the evaluation of other segmentation methods.

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